

Q1.

7	(a)		electrons fired at metal target	[5]
	(b)	(i)	increase cathode/tube currentB1	
		(ii)	increase anode voltageB1	
		(iii)	use aluminium filter (allow metal filter)	[3]
	(c)		$I = I_0 e^{-\mu x}$	[3]
Q2.				
8	(a)		produces greater intensity (at focus) limits region of cell damage allows for accurate guidance	[2]
	(b)		laser beam cauterises tissue can produce coagulation vaporisation of water in cells	[2]
Q3.			The same of the sa	
9	(a)		ability to detect (small) changes in loudness/intensity	[2]
	(b)		$\Delta I.L = 10 \lg(\Delta I/I) \text{ or } I.L = 10 \lg(I/I_0).$ C1 3.6 10 $\lg(I_2/(4.5 \times 10^{-5}).$ C1 $I_2 = 9.0 \times 10^{-5} \text{ Wm}^{-2}, \Delta I = 4.5 \times 10^{-5} \text{ W m}^{-2}.$ A1	[3]

Q4.



(a) X-ray beam directed through body onto detector (plate) different tissues absorb/attenuate beam by different amounts giving 'shadow' image of structures any other detail e.g. comment re sharpness or contrast	B1 B1 B1 B1	[4]
(b) X-ray image is flat OR 2-dimensional (1) CT scan takes many images of a slice at different angles (1) these build up an image of a slice through the body (1) series of images of slices is made (1) so that 3D image can be built up (1) image can then be rotated (1) 1 mark for each point, max 5	B5	[5]
large / strong (constant) magnetic field nuclei rotate about direction of field / precess radio frequency / r.f. pulse causes resonance in nuclei , nuclei absorb energy (pulse) is at the Larmor frequency on relaxation / nuclei de-excite emit (pulse of) r.f. detected and processed non-uniform field (superimposed) allows for position of nuclei to be determined and for location of detection to be changed (1) (B6 plus any two extra details, 1 each, max 2)	B1 B1 B1 B1 B1 B1 B2	[8]
(a) <u>pulse</u> of ultrasound reflected at boundaries / boundary received / detected (at surface) by transducer signal processed and displayed (1) time between transmission and receipt of pulse gives (information about) depth of boundary (1) reflected intensity gives information as to nature of boundary (1) (any four points, 1 each, max 4) (b) (i) coefficient = (Z ₂ - Z ₁) ² / (Z ₂ + Z ₁) ² = (6.3 - 1.7) ² / (6.3 + 1.7) ² = 0.33 (unit quoted, then -1) (ii) fraction = exp(-\(\mu x\)) = exp(-23 \times 4.1 \times 10^{-2}) = 0.39 (iii) intensity = 0.33 \times 0.39 ² \times I = 0.050 I (do not allow e.c.f. from (i) and (ii) if these answers are greater than 1)	B4 C1 A1 C1 A1 C1 A1	[4] [2] [2]
	different tissues absorb/attenuate beam by different amounts giving 'shadow' image of structures any other detail e.g. comment re sharpness or contrast (b) X-ray image is flat OR 2-dimensional (1) CT scan takes many images of a slice at different angles (1) these build up an image of a slice through the body (1) series of images of slices is made (1) so that 3D image can be built up (1) image can then be rotated (1) 1 mark for each point, max 5 large / strong (constant) magnetic field nuclei rotate about direction of field / precess (1) radio frequency / r.f. pulse causes resonance in nuclei, nuclei absorb energy (1) (pulse) is at the Larmor frequency (1) on relaxation / nuclei de-excite emit (pulse of) r.f. detected and processed non-uniform field (superimposed) allows for position of nuclei to be determined and for location of detection to be changed (1) (166 plus any two extra details, 1 each, max 2) (a) pulse of ultrasound reflected (at surface) by transducer (1) signal processed and displayed time between transmission and receipt of pulse gives (information about) depth of boundary (1) reflected intensity gives information as to nature of boundary (1) reflected intensity gives information as to nature of boundary (1) (2) (2) (2) (2) (3) (4) (4) (4) (4) (4) (4) (4) (4) (4) (4	different tissues absorb/attenuate beam by different amounts giving 'shadow' image of structures B1 any other detail e.g. comment re sharpness or contrast B1 (b) X-ray image is flat OR 2-dimensional (1) CT scan takes many images of a slice at different angles (1) these build up an image of a slice through the body (1) series of images of slices is made (1) so that 3D image can be built up (1) image can then be rotated (1) 1 mark for each point, max 5 B5 large / strong (constant) magnetic field nuclei rotate about direction of field / precess (1) radio frequency / r.f. pulse causes resonance in nuclei , nuclei absorb energy (1) (pulse) is at the Larmor frequency (1) on relaxation / nuclei de-excite emit (pulse of) r.f. B1 detected and processed B1 allows for position of nuclei to be determined B1 allows for position of nuclei to be determined B1 and for location of detection to be changed (1) (B6 plus any two extra details, 1 each, max 2) B2 (a) pulse of ultrasound reflected at boundaries / boundary (1) received / detected (at surface) by transducer (1) signal processed and displayed (1) time between transmission and receipt of pulse gives (information about) depth of boundary (1) reflected intensity gives information as to nature of boundary (1) reflected intensity gives information as to nature of boundary (1) reflected intensity gives information as to nature of boundary (1) reflected intensity gives information as to nature of boundary (2) (2) (2) (2) (2) (2) (2) (2) (2) (2)

Q7.



10 (a) X-ray taken of slice / plane / section repeated at different angles images / data is processed combined / added to give (2-D) image of slice repeated for successive slices to build up a 3-D image image can be viewed from different angles / rotated	B1 B1 B1 B1 B1 B1 max 6	[6]
(b) (i) 16	A1	[1]
(ii) evidence of deducting 16 then dividing by 3 to give 3 2 6 5	C1 A1	[2]
Q8.	0	
opposite faces /two sides coated (with silver) to act as electrodes either molecular structure indicated or centres of (+) and (–) charge not coincident potential difference across crystal causes crystal to change shape alternating voltage (in US frequency range) applied across crystal causes crystal to oscillate / vibrate (crystal cut) so that it vibrates at resonant frequency (max 6)	B B B B B B B	1 1 1 1
Q9. 10 (a) product of density (of medium) and speed of sound (in the medium)	B1	[1]

(b) α would be nearly equal to 1 $\frac{1}{either}$ reflected intensity would be nearly equal to incident intensity $\frac{1}{either}$ reflected intensity would be small $\frac{1}{either}$ M1 $\frac{1}{either}$ Transmitted intensity would be small $\frac{1}{either}$ M1 $\frac{1}{eithe$

(c) (i)
$$\alpha = (1.7 - 1.3)^2 / (1.7 + 1.3)^2$$
 C1
= 0.018 A1 [2]

(ii) attenuation in fat =
$$\exp(-48 \times 2x \times 10^{-2})$$
 C1
0.012 = 0.018 $\exp(-48 \times 2x \times 10^{-2})$ C1
 $x = 0.42 \text{ cm}$ A1

Q10.

[3]



10	strong / large (uniform) magnetic field		B1	
	nuclei precess / rotate about field direction	(1)		
	radio frequency pulse		B1	
	at Larmor frequency	(1)		
	causes resonance / nuclei absorb energy		B1	
	on relaxation / de-excitation, nuclei emit r.f. pulse		B1	
	pulse detected and processed	(1)		
	non-uniform field superposed on uniform field		B1	
	allows position of resonating nuclei to be determined		B1	
	allows for location of detection to be changed	(1)		
	(six points, 1 each plus any two extra – max 8)	1/1/20		[8]

Q11.

11 (a) (i)	e.m. radiation produced whenever charged particle is accelerated electrons hitting target have distribution of accelerations	M1 A1	[2]
(ii)	$ \begin{array}{ll} \textit{either} & \textit{wavelength shorter/shortest for greater/greatest acceleration} \\ \textit{or} & \lambda_{\min} = \textit{hc/E}_{\max} \\ \textit{or} & \textit{minimum wavelength for maximum energy} \\ \textit{all electron energy given up in one collision/converted to single photon} \\ \end{array} $	B1 B1	[2]
(b) (i)	hardness measures the penetration of the beam greater hardness, greater penetration	C1 A1	[2]
(ii)	controlled by changing the anode voltage higher anode voltage, greater penetration/hardness	C1 A1	[2]
(c) (i)	long-wavelength radiation more likely to be absorbed in the body/less likely to penetrate through body	B1	[1]
(ii)	(aluminium) filter/metal foil placed in the X-ray beam	B1	[1]

Q12.

12	(a)	strong uniform (magnetic) field either aligns nuclei	M1	
		or gives rise to Larmor/resonant frequency in r.f. region non-uniform (magnetic) field either enables nuclei to be located	A1 M1	
		or changes the Larmor/resonant frequency	A1	[4]
	(b)	(i) difference in flux density = $2.0 \times 10^{-2} \times 3.0 \times 10^{-3} = 6.0 \times 10^{-5} \text{ T}$	A1	[1]
		(ii) $\Delta f = 2 \times c \times \Delta B$ = $2 \times 1.34 \times 10^8 \times 6.0 \times 10^{-5}$	C1	
		$= 2 \times 1.34 \times 10^{-1} \times 6.0 \times 10^{-1}$ $= 1.6 \times 10^{4} \text{ Hz}$	Δ1	[2]

Q13.



10	(a)	e.g. beam is divergent/obeys inverse square law
		absorption (in block)
		scattering (of beam in block)
		reflection (at boundaries)

(any two sensible suggestions, 1 each)

(b) (i)
$$I = I_0 \exp(-\mu x)$$

 $I_0/I = \exp(0.27 \times 2.4)$
= 1.9

A1

C₁

C₁

(ii)
$$I_0/I = \exp(0.27 \times 1.3) \times \exp(3.0 \times 1.1)$$

= 1.42 × 27.1
= 38.5

A1

[2]

(c) either much greater absorption in bone than in soft tissue or I_0/I much greater for bone than soft tissue

[1]

Q14.

10 (a) sharpness: how well the edges (of structures) are defined contrast: difference in (degree of) blackening between structures B1 B1 [2]

(b) e.g. scattering of photos in tissue/no use of a collimator/no use of lead grid large penumbra on shadow/large area anode/wide to am large pixel size

(any two sensible suggestions, 1 each)

B2 [2]

(c) (i) $I = I_0 e^{-\mu x}$ ratio = $\exp(-2.85 \times 3.5) / \exp(-0.98 \times 8.0)$ = $(4.65 \times 10^{-5}) / (5.00 \times 0^{-5})$ = 0.093

C1

(ii) either large difference (in intensities)
or ratio much less than 1.0
so good contrast

A1

[3]

(answer gives in (c)(ii) must be consistent with ratio given in (c)(i))

M1 A1 [2]

[2]

Q15.

10 (a) product of density and speed of sound / wave (density of medium and) speed of sound / wave in medium M1 A1

(b) if $(Z_1 - Z_2)$ is small, mostly transmission if $(Z_1 - Z_2)$ is large, mostly reflection (if 'mostly' not stated allow 1/2 marks for these first two marks) either reflection / transmission also depends on $(Z_1 + Z_2)$

M1 M1

B1

or intensity reflection coefficient = $(Z_1 - Z_2)^2 / (Z_1 + Z_2)^2$

A1 [3]

(c) e.g. smaller structures can be distinguished because better resolution at shorter wavelength / higher frequency

1 [2]



Q16.

	11	(a)	a) changing voltage changes energy / speed of <u>electrons</u> changing electron energy changes maximum X-ray photon energy A1						
		(b)	(i)	1.	loss of power / energy / intensity		B1	[1]	
				2.	intensity changes when beam not parallel decreases when beam is divergent		C1 A1	[2]	
			(ii)		to = $(\exp \{-2.9 \times 2.5\})$ / $(\exp \{-0.95 \times 6.0\})$ = 0.21 (min. 2 sig. fig.) Hues of both lengths incorrect by factor of 10^{-2} to give ratio of 0	0.985 scores 1	C1 A1 1 mark)	[2]	
Q1	7.								
9	(a) p	orodi	uct c	of density (of medium) and speed of sound (in medium)		B1	[1]	
	(b) difference in acoustic impedance							[2]	
	(r (reflectime	cted cted for r	ultrasound (directed into body) at boundary (between tissues) l pulse is) detected and processed eturn of echo gives (information on) depth f reflection gives information on tissue structures		B1 B1 B1	[5]	
Q1	8.								
1	1		any	furth	ge: (thin) slice (through structure) ner detail e.g. built up from many 'slices' / 3-D image age: 'shadow' image (of whole structure) / 2-D image	1	B1 B1 B1	[3]	
			thes repe to bu 3-D com	e imeated	age of slice taken from many different angles lages are combined (and processed) of for many different slices up a 3-D image ge can be rotated er required to store and process huge quantity of data of the store and process huge for the store and pr	(1) (1) (1) (1) (1) (1)	B5	[5]	

Q19.



11			T magnetic field applied along body (allow 'across') (1)	(4)	
	r.t. p	ulse	appliednydrogen nuclei / protons	(1)	
			ate		
			return to equilibrium state / after relaxation time		
			e) emitted		
			etected, processed and displayed		
			t frequency depends on magnetic field strength		
	calib	rate	d non-uniform field enables nuclei to be located	(1)	
	any	six p	points, one mark each	B6	[6]
				[Tota	l: 6]
Q20).				
10	(a)	(i)	e.m. radiation / photons is produced whenever a charged particle	0	
	, ,	. ,	is accelerated		
			wavelength depens on magnitude of acceleration		
			electrons have a distribution of accelerations		
			so continuous spectrum	A0	[3]
		(ii)	either when electron loses all its energy in one collision		
		1	or when energy of electron produces a single photon	B1	[1]
				D.4	
	(b)	(1)	parallel beam (in matter) $I = I_0 \exp(-\mu x)$	B1	
			$I = I_0 \exp(-\mu x)$ $I, I_0, (\mu) \text{ and } x \text{ explained}$	IVI I	[3]
			1, 1 ₀ , (μ) and x explained	A1	[9]
		(ii)	either low-energy photons absorbed (much) more readily		
			or low-energy photons (far) less penetrating	B1	
			low-energy photons do not contribute (p.X-ray image	B1	- 22
			low energy photons could cause its see damage	B1	[3]
			WALL WES	[Total:	: 10]
Q21			A •		
			W		
			in the second se		
			. 37		
			1		



10) (a	(i)	der	sity × speed of wave (in the medium)	B1	[1]
		(ii	ρ:	= $(7.0 \times 10^6) / 4100$ = 1700 kg m^{-3}	A1	[1]
	(b) (i)	<i>I</i> =	I_{T} + I_{R}	B1	[1]
		(ii)	1. 6	$\alpha = (0.1 \times 10^6)^2 / (3.1 \times 10^6)^2$ = 0.001	C1 A1	[2]
			2 . <i>a</i>	<i>α</i> ≈ 1	A1	[1]
	(c)	or	ther	very little transmission at an air-skin boundary (almost) complete transmission at a gel-skin boundary when wave travels in or out of the body no gel, majority reflection with gel, little reflection when wave travels in or out of the body	M1 M1 A1 (M1) (M1) (A1)	[3]
Q22	2.					
9	(a)	(i)	edge	es can be (clearly) distinguished	B1 [[1]
		(ii)		size of X-ray source / anode / target / aperture scattering of X-ray beam pixel size two, 1 each) er detail e.g. use of lead grid	B2 B1	[3]
	(b)	CT	scan:	age involves a <u>single</u> exposure exposure of a <u>slice</u> from many different angles for different slices	B1 M1 A1	

Q23.

11 (a) (i)
$$I/I_0 = \exp(-1.5 \times 2.9)$$
 C1 $= 0.013$ A1 [2] (ii) $I/I_0 = \exp(-4.6 \times 0.95)$ $= 0.013$ A1 [1] (b) attenuation (coefficients) in muscle and in fat are similar attenuation (coefficients) in bone and muscle / fat are different contrast depends on difference in attenuation B1 [3]

CT scan involves a (much) greater exposure

Q24.

B1

[4]



10	quartz/piezo-electric crystal			B1		
	p.d. across crystal causes	either or	centres of (+) and (-) charge to move crystal to change shape	B1		
	alternating p.d. (in ultrasound crystal cut to produce resonation when crystal made to vibrate	B1 B1 M1				
	alternating p.d. produced across the crystal					

Q25.

- 11 (a) sharpness: ease with which edges of structures can be seen B1 contrast: difference in degree of blackening between structures B1 [2]
 - (b) (i) $I = I_0 e^{-\mu x}$ C1 $I/I_0 = \exp(-0.20 \times 8)$ = 0.20 A1 [2]
 - (ii) $I/I_0 = \exp(-\mu_1 \times x_1) \times \exp(-\mu_2 \times x_2)$ (could be three terms) C1 $I/I_0 = \exp(-0.20 \times 4) \times \exp(-12 \times 4)$ C1 $I/I_0 = 6.4 \times 10^{-22}$ or $I/I_0 \approx 0$ A1 [3]
 - (c) (i) sharpness unknown/no B1 [1]
 - (ii) contrast good/yes (ecf from (b)) B1 [1]

Q26.

10 X-ray images taken from different angles / X-rays directed from different angles **B1** of one section/slice all images in the same plane (1)images combined to give image of section/slice **B1** images of successive sections/slices combined **B1** image formed using a computer image formed is 3D image (1)that can be rotated/viewed from different angles (1)(four B-marks plus any two additional marks) B₂ [6]

Q27.



10	(a)	background reading = 19						
	(b)	A = B = C = D = (Allo	5 9		A1 A1 A1 A1	[4]		
	(c)	(i)	either 5, 14 or 14, 5 (A+D, B+C or v.v.)		B1	[1]		
		(ii)	Three numbers and 'inside' number is 8 (B+D) Three numbers and 'outside' numbers are either 2,9 or 9,2 (A,C o	or <i>v.v.</i>)	B1 B1	[2]		
Q28.								
10	(a)		se (of ultrasound) duced by quartz / piezo-electric crystal	(1)	B1			
		refle	ected from boundaries (between media) ected pulse detected		B1 B1			
		sign	the ultrasound transmitter all processed and displayed ansity of reflected pulse gives information about the boundary	(1)	B1			
		time	e delay gives information about depth or B marks plus any two from the four, max. 6)	(1)	B2	[6]		
	(b)		rter wavelength aller structures resolved / detected (not more sharpness)		B1 B1	[2]		
	(c)	(i)	$I = I_0 e^{-\mu x}$ ratio = exp(-23 × 6.4 × 10 ⁻²) = 0.23		C1 C1 A1	[3]		
		(ii)	later signal has passed through greater thickness of medium so has greater attenuation / greater absorption / smaller intensi	ty	M1 A1	[2]		
Q29.								
10	(a)	spi	clei spin/precess n/precess about direction of magnetic field ner frequency of precession depends on magnetic field strength large field means frequency in radio frequency range		B1 B1	[3]		
	(b)	of s	n-uniform field means frequency of precession different in dif- subject ables location of precessing nuclei to be determined ables thickness of slice to be varied/location of slice to be change		B1 B1 B1	[3]		

Q30.



12 (8	t t r	taken from different angles to give image of the section/slice repeated for many slices	M1 M1 A1 M1 A1 [5]	
(t		12 N : 10 N : 1	C1 C1	
	F	P = 5 Q = 9 R = 7 S = 13		
	((four correct 2/2, three correct 1/2)	A2 [4]	
Q31.				
11	(a)	X-ray: flat/shadow/2D image regardless of depth of object/depth not indicated	B1 B1	
		CT scan: built up from (many) images at different angles image is three-dimensional	B1 B1	
		image can be rotated/viewed at different angles	B1 [5]	
	(b)	image is three-dimensional image can be rotated/viewed at different angles (i) $I = I_0 e^{-\mu x}$ $0.25 = e^{-0.69x}$ $x = 2.0 \text{ mm } (allow 1 \text{ s.f.})$ (ii) for aluminium, $I/I_0 = e^{-0.46 \times 2.4}$	C1	
		$x = 2.0 \mathrm{mm} (allow 1 s.f.)$	A1 [2]	
		(ii) for aluminium, $I/I_0 = e^{-0.46 \times 2.4}$ = 0.33 fraction = 0.33 × 0.25	C1	

Q32.

= 0.083

= 10 lg(0.083) = (-) 10.8 dB (allow 2 s.f.)

(iii) $gain/dB = 10lg(I/I_0)$

with negative sign

11	(a)	X-ray beam contains many wavelengths aluminium filter absorbs long wavelength X-ray radiation that would be absorbed by the body (and not contribute to the image)	M1 A1	[3]	
	(b)	CT scan consists of (many) X-ray <u>images</u> of a slice and there are many slices X-ray image is a single exposure (so much) greater exposure with CT scan	M1 A1 B1 B1	[4]	Q33.

[2]

[3]

A₁



11	(a)	product of density and speed	M1	
		density of medium, speed of wave in medium	A1	[2]
		(not "speed of light", 0/2)		

(b) (i)
$$\alpha = (6.4 - 1.7)^2/(6.4 + 1.7)^2$$
 C1
= 0.34 A1 [2]

(ii)
$$I/I_0 = e^{-\mu x}$$
 C1
= $\exp(-23 \times 3.4 \times 10^{-2})$ C1
= 0.46 A1 [3]

(iii)
$$I_R/I = (0.46)^2 \times 0.34$$
 C1
= 0.072 A1 [2]



whith the dale citalitie.